بِسْمِ اللهِ الرَّحْمَنِ الرَّحِيمِ

﴿ اقْرَأْ بِاسْمِ رَبِّكَ الَّذِي خَلَقَ *خَلَقَ الْإِنْسَانَ مِنْ عَلَقٍ *اقْرَأْ وَرَبُّكَ الْأَكْرَمُ *الَّذِي عَلَّمَ بِالْقَلَمِ *عَلَّمَ الْإِنْسَانَ مَا لَمْ يَعْلَمْ ﴾

Dedication

To my lovely family and wonderful mother's for her love and support, to my husband Hindi Abd AL Hafez for raising me in a way to believe that I can achieve anything in life with hard work, and dedication to my twins (Judy and Jana), and to everybody who helps me in this work.

ACKNOWLEDGEMENTS

In the name of ALLAH the most Merciful the most Compassionate, I would like first and foremost give thanks to our LORD for all HE has given us and for it is in his name that we go further.

I am greatly indebted to my supervisor Dr. Zeinab Adam Mustafa, for her guidance, advice and constant support throughout my thesis work, who generously shares her knowledge and experience with all her students. I really appreciate her ultimate help, personal concern, patient and objective support.

In addition, All my thanks and wishes to Eng. Mohamed El-Tahir for his help and friendly attitude.

Most importantly, I wish to thank my loving and supportive brothers, sisters and friends.

Abstract

Electrocardiogram (ECG)is one of the most important techniques that used for diagnosing cardiac arrhythmias. Automatic detection and classification of ECG signals is paramount since scrutinizing each and every beat is a tedious job specially when we need to record the heart's electrical activity versus time, this is tediousness leads to increase the human error factor in the cardiologist decisions. In this research, have been used an accurate method of classification and differentiation of Normal and abnormal heartbeats.

1500ECG signals were collected from MIT-BIH Arrhythmia database in Physionet bank in Physionet website. 1000 of these signals are said to be abnormal and the rest 500 signals are normal sinus rhythm ECG. These signals were processed to remove baseline wonder and high frequency noise using band path filter.

The Matlab program was also developed to extract the main feature of the ECG signals during a set period of time. 10 features were extracted and divided into 2 groups: ECG features and statistical features, All the features were presented in an excel file and used in the development of the ANN. the signal has been segmented into smaller samples then detecting the R peak knowing that it is the easiest feature to detect because it's the highest peak. The rest of the features were collected easily once R peak is known. Artificial Neural Network was used in the classification step. The normal signal was given the number 1 while the abnormal sample was 0 in the construction of ANN. All these data were used in the training of ANN and the results was collected and discussed. The system successfully classified and differentiate between the normal and abnormal with accuracy 99.7%, and between atrial premature beat(APB) and paced beat(PB) with accuracy 95.1%.

الخلاصة

قياس كهربية القلب أو ما يعرف بتخطيط القلب يعد من أهم التقنيات التي تستخدم لتشخيص اضطراب ضربات القلب. فمن المهم وجود أنظمة ذكية قادرة على قراءة وتمييز إشارات رسم القلب وذلك لأن عملية تشخيص وقراءة رسم القلب عملية مملة ومرهقة خصوصا عندما يتطلب الأمر إجراء ومتابعة رسم القلب للمرضى عدة مرات خلال اليوم الواحد، هذا قد يقود إلى زيادة عامل الخطأ الشخصي مما يؤدي إلى اتخاذ قرارات خاطئة في التشخيص.

في هذا البحث تم استخدام طريقة دقيقة للتمييز والتفريق بين إشارات القلب الطبيعية وغير الطبيعية, وبين زيادة ضربات القلب ونقصان ضربات القلب.

تم تجميع 1500 إشارات رسم قلب كهربائية من موقع فيزيونت الالكتروني, 1000 من هذه الإشارات تعتبر غير طبيعيه وباقي 500 إشارة هي عبارة عن إشارات ذات نمط طبيعي. وعولجت هذه الإشارات لإزالة التشويش والذبذبات ذات التردد العالي باستخدام تقنية مرشح ممر الموجة.

تم تطوير برنامج ماتلاب ليقوم باستخراج المميزات الأساسية لإشارة رسم القلب خلال فترة زمنيه محددة, وتم استخراج 10 مميزات وقسمت إلى مجموعتان هما : مميزات قياس كهربية القلب ومميزات إحصائية. وقد تم تجميع كل هذه المميزات في ملف اكسل ليتم استخدامه في إنشاء الشبكة العصبية . وتم تقسيم الإشارة إلى عينات اصغر ومن ثم البحث عن القمة R مع العلم أنها أسهل مميزة يتم اكتشافها لأنها اعلى قمة, باقي المميزات تم تجميعها بسهولة بمجرد معرفة موقع القمة R.

واستخدمت الشبكة العصبية الاصطناعية في مرحلة التصنيف, وتم إعطاء الإشارات الطبيعية الرقم 1 والإشارات غير الطبيعية الرقم 0 في تصميم الشبكة العصبية. كل هذه المعلومات تم استخدامها لتدريب الشبكة وتم تحصيل النتائج ومناقشتها. وبلغت دقة هذا النظام 99.7% بين الإشارات الطبيعية وغير الطبيعية,و 95.1% بين زيادة ضربات القلب ونقصان ضربات القلب.

Contents

I
DedicationII
AcknowledgementIII
AbstractIV
الخلاصة الخلاصة
List of tablesX
List of figuresX
List of AcronymsXIII
CHAPTER 1: INTRODUCTION
1.1 General View
1.2 Problem Statement
1.3 Thesis Objectives
1.3.1main objective
1.3.2Specific objective
1.4 Methodology
1.5 Thesis Layout4
CHAPTER 2: Literature Review
2.1 Classification of ECG Arrhythmias Using Discrete Wavelet Transform and Neural
Networks5
2.2 A novel Approach for Classification of ECG Arrhythmias: type-2 fuzzy clustering neural
network6
2.3 Automated Detection of Arrhythmias Using Different Intervals of Tachycardia ECG
Segments With Convolutional Neural Network7

2.4 Automatic Classification of ECG Signals With Features Extracted Using Wavelet Transform
and Support Vector Machines8
2.5 Classification of ECG Arrhythmias Using Adaptive Neuro-fuzzy Inference System and
Cuckoo Optimization Algorithm9
2.6 Detection of Ventricular Fibrillation Using Hilbert Transforms, Phase-space reconstruction,
and Time-domain analysis9
2.7 ECG Beats Classification Using Mixture of Features
2.8 Novel ECG Signal Classification Based on KICA Nonlinear Feature Extraction11
2.9 Optimization of ECG Classification By Means of Feature Selection
2.10 A Multi-stage Neural Network Classifier For ECG Events
2.11 Wavelet/Mixture of Experts Network Structure for EEG Signals Classification
2.12 ECG Beat Classification Using Neuro-fuzzy Network
2.13 Analysis of ECG signal for Detection of Cardiac Arrhythmias
2.14 Analysis of Electrocardiograph (ECG) Signal for the Detection of Abnormalities Using
MATLAB16
2.15 Application of Artificial Neural and Fuzzy-Neural Networks to QRS Detection and PVC
Diagnosis
2.16 Matlab implementation of ECG signal processing
Chapter 3: THEORATICAL BACKGROUND
3.1 Heart Anatomy
3.2 Normal Heart Function and the Electrophysiology of the Heart20
3.3 Electrocardiogram

3.3.1 ECG Leads	23
3.3.2 Colors in ECG	27
3.3.3 ECG Waves and Intervals	28
3.3.4 ECG Noise	29
3.3.4.1 Power Line Interference	30
3.3.4.2 Electrodes Contact Noise and Motion Artifacts	32
3.3.4.3 EMG Noise	34
3.3.4.4 Instrumentation Noise	34
3.4 Arrhythmias in ECG signal	35
3.5 Artificial Neural Networks (ANNs)	
3.5.1 General Overview Of Artificial neural networks	36
3.5.2 Basic Architecture of a feed-forward networks	40
3.5.3 ANNs training and generalization	40
3.5.4 Network coupled Errors	41
CHAPTER 4: METHODOLOGY	
4 Methodology	42
4.1Preprocessing Module	43
4.1.1 Used Signals	43
4.1.2 Band Pass Filter	46
4.2 Feature Extraction Module	47
4.2.1 R Peak Detection	47
4.2.2 P, Q, S and T Detection	48
4.2.3 statistical features	49
4.3 features selection and reduction	49
4.4 Classifier and Optimizer Module	49
4.4.1 Artificial Naural Natural	40

4.5 Output Module	52
CHAPTER 5: RESULTS AND DISCUSSION	
5.1 ECG Data	53
5.2 Main Window	53
5.3 results between normal signals and abnormal	55
5.4 results between a trial premature beat and paced beat	60
5.5 discussion.	64
CHAPTER 6: CONCLUSION AND RECOMMENDATIONS	
6.1Conclusion.	65
6.2 Recommendations	65
Reference	66
Appendix	70

List of Tables

Table	Description	Page
No.		No.
Table 3-1	Shows the types of leads used in ECG monitoring	24
Table 3-2	Shows the features of P-wave, QRS complex and T wave	28

List of Figures

Figure	Description	Page
No.		No.
Figure 3-1	Shows the Heart conduction system.	20
Figure 3-2	Shows the ideal ECG signal.	21
Figure 3-3	Shows the ECG leads.	25
Figure 3-4	Shows the schematic representation of normal ECG wave form.	27
Figure 3-5	Shows the block diagram of principal noise source in ECG.	30
Figure 3-6	Shows the Fourier power spectrum of ECG trace.	31
Figure 3-7	Shows the seventy seconds of ECG data.	32
Figure 3-8	Shows the two seconds of ECG trace.	34
Figure 3-9	Shows the biological neuron.	38
Figure 3-10	Shows the architecture structure of feed forward network.	39
Figure 3-11	Shows the errors vs. optimal network training time.	41
Figure 4-1	Shows the block diagram of proposed method of ECG classification.	43
Figure 4-2	Normal signal	44
Figure 4-3	A trial premature beat signal	45

Figure 4-4	Paced beat signal	46
Figure 4-5	Shows the main window of the tools which is open using (nprtool).	51
Figure 4-6	Shows the window show where to input the feature elements and the targets for classifications.	51
Figure 5-1	Shows the : Neural Network Training Window (nntaintool).	54
Figure 5-2	Shows the confusion window.	55
Figure 5-3	Shows the retraining window.	56
Figure 5-4	Shows the second confusion window.	57
Figure 5-5	Shows the Receiver Operating Characteristics (plotroc)(ROC).	58
Figure 5-6	Shows the Performance (plotperform).	59
Figure 5-7	Shows the training state	59
Figure 5-8	Shows the confusion window(APB&PB).	60
Figure 5-9	Shows the Receiver Operating Characteristics (plotroc)(ROC)(APB &PB).	61
Figure 5-10	Shows the Performance (plotperform)(APB&PB).	62
Figure 5-11	Shows the training state(APB&PB)	62
Figure 5-12	Shows the Neural Network Pattern Recognition Tool	63

List of Acronyms

Acronyms	Stand For
ECG	Electro Cardio Gram
ANNs	Artificial neural networks
N	Normal
PB	Paced beat
APB	Atrial premature beat
EMG	Electromyography
SNR	Signal to noise ratio
SA	Sino atrial
LBBB	Left bundle branch block
RBBB	right bundle branch block
APC	Atrial premature contractions
PVC	Premature ventricular contractions
T2FCM	Type-2 fuzzy c-means clustering
AAMI	Advancement of medical instrumentation

MLP	Multilayer perceptron
DOM	Difference operation method
RBF	Radial basis function
DWT	Discrete wave transform
MATLAB	Matrix laboratory
SVM	Support victor machine
KICA	Kernel independent component analysis
OAO	One against one
PCA	Principal component analysis
SFFS	Sequential forward floating search
KNN	k-nearest neighbor